

(19)



Europäisches Patentamt  
European Patent Office  
Office européen des brevets



(11)

**EP 1 428 524 A1**

(12)

**EUROPEAN PATENT APPLICATION**

(43) Date of publication:  
**16.06.2004 Bulletin 2004/25**

(51) Int Cl.7: **A61K 9/00, A61K 9/16**

(21) Application number: **04075809.6**

(22) Date of filing: **12.04.1996**

(84) Designated Contracting States:  
**AT BE CH DE DK ES FI FR GB GR IE IT LI LU MC  
NL PT SE**

(30) Priority: **14.04.1995 US 423515**

(62) Document number(s) of the earlier application(s) in  
accordance with Art. 76 EPC:  
**96911738.1 / 0 825 885**

(71) Applicant: **Nektar Therapeutics**  
**San Carlos, CA 94070-6256 (US)**

(72) Inventors:  
• **Platz, Robert M.**  
**Half Moon Bay, CA 94019 (US)**

• **Platton, John S.**  
**San Carlos, CA 94070 (US)**  
• **Foster, Linda**  
**Sunnyvale, CA 94086 (US)**  
• **Eljamal, Mohammed**  
**San Jose, CA 95129 (US)**

(74) Representative: **Baldock, Sharon Claire et al**  
**BOULT WADE TENNANT,**  
**Verulam Gardens**  
**70 Gray's Inn Road**  
**London WC1X 8BT (GB)**

Remarks:

This application was filed on 15 - 03 - 2004 as a  
divisional application to the application mentioned  
under INID code 62.

(54) **Pulmonary delivery of aerosolized medicaments**

(57) The invention provides a spray-dried pharmaceutical-based dispersible dry powder composition for pulmonary delivery, comprising: a therapeutically effective amount of a macromolecule; and a pharmaceutically acceptable carrier with the provisos that: (i) the carrier

is neither hydroxypropylcellulose or hydroxypropylmethylcellulose; and (ii) the macromolecule is neither insulin nor an interferon.

**EP 1 428 524 A1**

## Description

## BACKGROUND OF THE INVENTION

## 1. Field of the Invention.

[0001] The present invention relates generally to methods and compositions for the dry powder formulation of pharmaceuticals, including macromolecules, for pulmonary delivery.

[0002] Over the years, certain drugs have been sold in compositions suitable for forming a drug dispersion for oral inhalation (pulmonary delivery) to treat various conditions in humans. Such pulmonary drug delivery compositions are designed to be delivered by inhalation by the patient of a drug dispersion so that the active drug within the dispersion can reach the lung. It has been found that certain drugs delivered to the lung are readily absorbed through the alveolar region directly into blood circulation. Pulmonary delivery is particularly promising for the delivery of macromolecules (proteins, polypeptides and nucleic acids) which are difficult to deliver by other routes of administration. Such pulmonary delivery can be effective both for systemic delivery and for localized delivery to treat diseases of the lungs.

[0003] Pulmonary drug delivery can itself be achieved by different approaches, including liquid nebulizers, aerosol-based metered dose inhalers (MDI's), and dry powder dispersion devices. Aerosol-based MDI's are losing favor because they rely on the use of chlorofluorocarbons (CFC's), which are being banned because of their adverse effect on the ozone layer. Dry powder dispersion devices, which do not rely on CFC aerosol technology, are promising for delivering drugs that may be readily formulated as dry powders. Many otherwise labile macromolecules may be stably stored as lyophilized or spray-dried powders by themselves or in combination with suitable powder carriers. The ability to deliver pharmaceutical compositions as dry powders, however, is problematic in certain respects. The dosage of many pharmaceutical compositions is often critical so it is necessary that any dry powder delivery system be able to accurately, precisely, and reliably deliver the intended amount of drug. Moreover, many pharmaceutical compositions are quite expensive. Thus, the ability to efficiently deliver the dry powders with a minimal loss of drug is critical. It is also essential that the powder be readily dispersible prior to inhalation by the patient in order to assure adequate distribution and systemic absorption.

[0004] A particularly promising approach for the pulmonary delivery of dry powder drugs utilizes a hand-held device with a hand pump for providing a source of pressurized gas. The pressurized gas is abruptly released through a powder dispersion device, such as a venturi nozzle, and the dispersed powder made available for patient inhalation. While advantageous in many respects, such hand-held devices are problematic in a number of other respects. The particles being delivered are less than 10  $\mu\text{m}$  in size, usually in the range from 1  $\mu\text{m}$  to 5  $\mu\text{m}$ , making powder handling and dispersion more difficult than with larger particles. The problems are exacerbated by the relatively small volumes of pressurized gas, which are available using hand-actuated pumps. In particular, venturi dispersion devices are unsuitable for difficult-to-disperse powders when only small volumes of pressurized gas are available. Another requirement for hand-held and other powder delivery devices is efficiency. It is important that the concentration of drug in the bolus of gas be relatively high to reduce the number of breaths required to achieve a total dosage. The ability to achieve both adequate dispersion and small dispersed volumes is a significant technical challenge that requires in part that each unit dosage of the powder composition be readily and reliably dispersible. Powdered compositions comprising macromolecules for inhalation are described in WO 91/16038 and EPA-611567.

## SUMMARY OF THE INVENTION

[0005] According to the subject invention, dispersible dry powder pharmaceutical-based compositions are provided, including methods for their manufacture and dry powder dispersion devices. A dispersible dry powder pharmaceutical-based composition is one having a moisture content of less than about 10% by weight (%w) water, usually below about 5%w and preferably less than about 3%w; a particle size of about 1.0-5.0  $\mu\text{m}$  mass median diameter (MMD), usually 1.0-4.0  $\mu\text{m}$  MMD, and preferably 1.0-3.0  $\mu\text{m}$  MMD; a delivered dose of about >30%, usually >40%, preferably >50%, and most preferred >60%; and an aerosol particle size distribution of about 1.0-5.0  $\mu\text{m}$  mass median aerodynamic diameter (MMAD), usually 1.5-4.5  $\mu\text{m}$  MMAD, and preferably 1.5-4.0  $\mu\text{m}$  MMAD. Such compositions are of pharmaceutical grade purity.

## DESCRIPTION OF SPECIFIC EMBODIMENTS

[0006] The present invention is based at least in part on the dispersibility characteristics of the pharmaceutical-based dry powder compositions produced according to the present invention. The dispersibility characteristics of the subject pharmaceutical-based compositions means that they are more suitable for use in pulmonary delivery devices than compositions prepared by other methods. The compositions of the invention are readily aerosolized and rapidly ab-

sorbed through the lungs of a host when delivered by a dry powder inhaler.

## DEFINITIONS

5 [0007] In interpreting the claims to the various aspects of this invention, there are several important definitions that should be considered.

[0008] The term "dispersibility" or "dispersible" means a dry powder having a moisture content of less than about 10% by weight (%w) water, usually below about 5%w and preferably less than about 3%w; a particle size of about 1.0-5.0  $\mu\text{m}$  mass median diameter (MMD), usually 1.0-4.0  $\mu\text{m}$  MMD, and preferably 1.0-3.0  $\mu\text{m}$  MMD; a delivered dose of about >30%, usually >40%, preferably >50%, and most preferred >60%; and an aerosol particle size distribution of about 1.0-5.0  $\mu\text{m}$  mass median aerodynamic diameter (MMAD), usually 1.5-4.5  $\mu\text{m}$  MMAD, and preferably 1.5-4.0  $\mu\text{m}$  MMAD.

[0009] The term "powder" means a composition that consists of finely dispersed solid particles that are free flowing and capable of being readily dispersed in an inhalation device and subsequently inhaled by a subject so that the particles reach the lungs to permit penetration into the alveoli. Thus, the powder is said to be "respirable." Preferably the average particle size is less than about 10 microns ( $\mu\text{m}$ ) in diameter with a relatively uniform spheroidal shape distribution. More preferably the diameter is less than about 7.5  $\mu\text{m}$  and most preferably less than about 5.0  $\mu\text{m}$ . Usually the particle size distribution is between about 0.1  $\mu\text{m}$  and about 5  $\mu\text{m}$  in diameter, particularly about 0.3  $\mu\text{m}$  to about 5  $\mu\text{m}$ .

20 [0010] The term "dry" means that the composition has a moisture content such that the particles are readily dispersible in an inhalation device to form an aerosol. This moisture content is generally below about 10% by weight (%w) water, usually below about 5%w and preferably less than about 3%w.

[0011] The term "therapeutically effective amount" is the amount present in the composition that is needed to provide the desired level of drug in the subject to be treated to give the anticipated physiological response. This amount is determined for each drug on a case-by-case basis. Guidelines are given hereafter.

25 [0012] The term "physiologically effective amount" is that amount delivered to a subject to give the desired palliative or curative effect. This amount is specific for each drug and its ultimately approved dosage level. Guidelines are given hereafter.

[0013] The term "pharmaceutically acceptable carrier" means that the carrier can be taken into the lungs with no significant adverse toxicological effects on the lungs.

## COMPOSITIONS OF THE INVENTION

35 [0014] One aspect of this invention is a dispersible pharmaceutical-based dry powder composition for pulmonary delivery, the composition comprising a therapeutically effective amount of a pharmaceutical in combination with a pharmaceutically acceptable carrier.

[0015] In general, the compositions of this invention are suitable for pulmonary delivery because of their dispersibility characteristics. Such compositions were not previously known in the art. In the dry state, the pharmaceutical may be in crystalline or amorphous form. Some examples of pharmaceutical compositions suitable for formulation into dispersible dry powders are listed in Table 1. These include macromolecule and non-macromolecule-based pharmaceuticals, usually macromolecules, with insulin, interleukin-1 receptor, parathyroid hormone (PTH-34), alpha-1 antitrypsin, calcitonin, low molecular weight heparin, heparin, interferon, and nucleic acids being preferred.

45 [0016] A therapeutically effective amount of active pharmaceutical will vary in the composition depending on the biological activity of the drug employed and the amount needed in a unit dosage form. Because the subject compounds are dispersible, it is highly preferred that they be manufactured in a unit dosage form in a manner that allows for ready manipulation by the formulator and by the consumer. This generally means that a unit dosage will be between about 0.5 mg and 15 mg of total material in the dry powder composition, preferably between about 2 mg and 10 mg. Generally, the amount of drug in the composition will vary from about 0.05%w to about 99.0%w. Most preferably the composition will be about 0.2% to about 97.0%w drug.

50 [0017] The amount of the pharmaceutically acceptable carrier is that amount needed to provide the necessary stability, dispersibility, consistency and bulking characteristics to ensure a uniform pulmonary delivery of the composition to a subject in need thereof. Numerically the amount may be from about 0.05%w to about 99.95%w, depending on the activity of the drug being employed. Preferably about 5%w to about 95%w will be used.

55 [0018] The carrier may be one or a combination of two or more pharmaceutical excipients, but will generally be substantially free of any "penetration enhancers." Penetration enhancers are surface active compounds which promote penetration of a drug through a mucosal membrane or lining and are proposed for use in intranasal, intrarectal, and intravaginal drug formulations. Exemplary penetration enhancers include bile salts, e.g., taurocholate, glycocholate, and deoxycholate; fusidates, e.g., taurodehydrofusidate; and biocompatible detergents, e.g., Tweens, Laureth-9, and

the like. The use of penetration enhancers in formulations for the lungs, however, is generally undesirable because the epithelial blood barrier in the lung can be adversely affected by such surface active compounds. The dry powder compositions of the present invention are readily absorbed in the lungs without the need to employ penetration enhancers.

[0019] The types of pharmaceutical excipients that are useful as carriers in this invention include stabilizers such as human serum albumin (HSA), bulking agents such as carbohydrates, amino acids and polypeptides; pH adjusters or buffers; salts such as sodium chloride; and the like. These carriers may be in a crystalline or amorphous form or may be a mixture of the two.

[0020] It has been found that HSA is particularly valuable as a carrier in that it provides improved dispersibility.

[0021] Bulking agents that are particularly valuable include compatible carbohydrates, polypeptides, amino acids or combinations thereof. Suitable carbohydrates include monosaccharides such as galactose, D-mannose, sorbose, and the like; disaccharides, such as lactose, trehalose, and the like; cyclodextrins, such as 2-hydroxypropyl- $\beta$ -cyclodextrin; and polysaccharides, such as raffinose, maltodextrins, dextrans, and the like; alditols, such as mannitol, xylitol, and the like. A preferred group of carbohydrates includes lactose, trehalose, raffinose maltodextrins, and mannitol. Suitable polypeptides include aspartame. Amino acids include alanine and glycine, with glycine being preferred.

[0022] Additives, which are minor components of the composition of this invention, may be included for conformational stability during spray drying and for improving dispersibility of the powder. These additives include hydrophobic amino acids such as tryptophan, tyrosine, leucine, phenylalanine, and the like.

[0023] Suitable pH adjusters or buffers include organic salts prepared from organic acids and bases, such as sodium citrate, sodium ascorbate, and the like; sodium citrate is preferred.

[0024] The unit dosage form, method of treatment, and process of preparation of this invention are described hereafter.

#### Unit Dosage Form.

[0025] Another aspect of this invention is a unit dosage form for pulmonary delivery of dispersible dry powder pharmaceutical-based compositions, which dosage form comprises a unit dosage receptacle containing a pharmaceutical-based dry powder composition, which composition comprises a therapeutically effective amount of a pharmaceutical in combination with a pharmaceutically acceptable carrier.

[0026] In this aspect of the invention, the composition of this invention (as discussed hereinbefore) is placed within a suitable dosage receptacle in an amount sufficient to provide a subject with drug for a unit dosage treatment. The dosage receptacle is one that fits within a suitable inhalation device to allow for the aerosolization of the interferon-based dry powder composition by dispersion into a gas stream to form an aerosol and then capturing the aerosol so produced in a chamber having a mouthpiece attached for subsequent inhalation by a subject in need of treatment. Such a dosage receptacle includes any container enclosing the composition known in the art such as gelatin or plastic capsules with a removable portion that allows a stream of gas (e.g., air) to be directed into the container to disperse the dry powder composition. Such containers are exemplified by those shown in U.S. Patents 4,227,522 issued October 14, 1980; 4,192,309 issued March 11, 1980; and 4,105,027 issued August 8, 1978. Suitable containers also include those used in conjunction with Glaxo's Ventolin Rotohaler brand powder inhaler or Fison's Spinhaler brand powder inhaler. Another suitable unit-dose container which provides a superior moisture barrier is formed from an aluminum foil plastic laminate. The pharmaceutical-based powder is filled by weight or by volume into the depression in the formable foil and hermetically sealed with a covering foil-plastic laminate. Such a container for use with a powder inhalation device is described in U.S. Patent 4,778,054 and is used with Glaxo's Diskhaler® (U.S. Patents 4,627,432; 4,811,731; and 5,035,237). All of these references are incorporated herein by reference.

#### Method of Treating a Disease State.

[0027] Another aspect of this invention is a method of treating a condition responsive to treatment by a pharmaceutical of interest, which method comprises pulmonarily administering to a subject in need thereof a physiologically effective amount of a dispersible pharmaceutical-based dry powder composition that comprises a therapeutically effective amount of drug in combination with a pharmaceutically acceptable carrier.

[0028] Conditions that may be treated by the compositions of this are described in Table 1.

[0029] The physiologically effective amount needed to treat a particular condition or disease state will depend on the individual, the condition, the length of treatment, the regularity of treatment, the type of drug, and other factors, but can be determined by one of ordinary skill in the medicinal arts.

[0030] It is presently believed that the effective absorption by a host of a dry powder composition according to the present invention results from a rapid dissolution in the ultra-thin (<0.1  $\mu$ m) fluid layer of the alveolar lining of the lung. The particles of the present invention thus have a mean size which is from 10 to 50 times larger than the lung fluid

layer, making it unexpected that the particles are dissolved and the interferon systemically absorbed in a rapid manner for either local lung or systemic treatment. An understanding of the precise mechanism, however, is not necessary for practicing the present invention as described herein.

[0031] The aerosolized pharmaceutical-based dry powders of this invention are particularly useful in place of parenteral delivery. Thus, the methods and compositions of the present invention will be particularly valuable in chronic treatment protocols where a patient can self-medicate. The patient can achieve a desired dosage by inhaling an appropriate amount of drug, as just described. The efficiency of systemic delivery via the method as just described will typically be in the range from about 15% to 50%.

#### Method for Aerosolizing the Powder.

[0032] Still another aspect of this invention is a device and method for aerosolizing a pharmaceutical-based dry powder composition that comprises a therapeutically effective amount of drug in combination with a pharmaceutically acceptable carrier, which method comprises dispersing an amount of the dry powder composition in a gas stream to form an aerosol and capturing the aerosol in a chamber having a mouthpiece for subsequent inhalation by a patient.

[0033] A further detailed description of this method is found in pending U.S. Patent Application Serial Nos.: 07/910,048 and 08/207,472, both of which are incorporated herein by reference.

#### Preparing the Compositions.

[0034] Still another aspect of this invention is a method for preparing a dispersible pharmaceutical-based dry powder composition of this invention that comprises spray drying an aqueous mixture of the drug and a pharmaceutically acceptable carrier under conditions to provide a respirable dry powder composition.

[0035] Spray drying is a process in which a homogeneous aqueous mixture of drug and the carrier is introduced via a nozzle (e.g., a two fluid nozzle), spinning disc or an equivalent device into a hot gas stream to atomize the solution to form fine droplets. The aqueous mixture may be a solution, suspension, slurry, or the like, but needs to be homogeneous to ensure uniform distribution of the components in the mixture and ultimately the powdered composition. Preferably the aqueous mixture is a solution. The solvent, generally water, rapidly evaporates from the droplets producing a fine dry powder having particles 1 to 5  $\mu\text{m}$  in diameter. Surprisingly, the drug is not degraded when it is exposed to the hot drying gas, and the interferon powders can be prepared having sufficient purity for pharmaceutical use. An acceptable purity is defined as less than 5% degradation products and contaminants, preferably less than 3% and most preferably less than 1%.

[0036] The spray drying is done under conditions that result in substantially amorphous powder of homogeneous constitution having a particle size that is respirable, a low moisture content and flow characteristics that allow for ready aerosolization. Preferably the particle size of the resulting powder is such that more than about 98% of the mass is in particles having a diameter of about 10  $\mu\text{m}$  or less with about 90% of the mass being in particles having a diameter less than 5  $\mu\text{m}$ . Alternatively, about 95% of the mass will have particles with a diameter of less than 10  $\mu\text{m}$  with about 80% of the mass of the particles having a diameter of less than 5  $\mu\text{m}$ .

[0037] The solutions may then be sprayed dried in conventional spray drying equipment from commercial suppliers, such as Buchi, Niro, Yamato Chemical Co., Okawara Kakoki Co., and the like, resulting in a substantially amorphous particulate product.

[0038] For the spraying process, such spraying methods as rotary atomization, pressure atomization and two-fluid atomization can be used. Examples of the devices used in these processes include "Parubisu [phonetic rendering] Mini-Spray GA-32" and "Parubisu Spray Drier DL-41", manufactured by Yamato Chemical Co., or "Spray Drier CL-8," "Spray Drier L-8," "Spray Drier FL-12," "Spray Drier FL-16" or "Spray Drier FL-20," manufactured by Okawara Kakoki Co., can be used for the method of spraying using rotary-disk atomizer.

[0039] While no special restrictions are placed on the nozzle of the atomizer used in the process of spraying, it is recommended to use a nozzle which can produce a spray-dry composition with a grain diameter suitable for nasal, pharyngeal or pulmonary administration. For example, nozzle types "1A," "1," "2A," "2," "3" and the like, manufactured by Yamato Chemical Co., can be used for the above-mentioned spray-drier, manufactured by the same company. In addition, disks type "MC-50," "MC-65" or "MC-85," manufactured by Okawara Kakoki Co., can be used as rotary disks of the spray-drier atomizer, manufactured by the same company.

[0040] While no particular restrictions are placed on the gas used to dry the sprayed material, it is recommended to use air, nitrogen gas or an inert gas. The temperature of the inlet of the gas used to dry the sprayed materials such that it does not cause heat deactivation of the sprayed material. The range of temperatures may vary between about 50°C to about 200°C, preferably between about 50°C and 100°C. The temperature of the outlet gas used to dry the sprayed material, may vary between about 0°C and about 150°, preferably between 0°C and 90°C, and even more preferably between 0°C and 60°C. The fact that inlet and outlet temperatures above about 55°C can be used is sur-

prising in view of the fact that most macromolecule-based drugs deactivate at that temperature, with nearly complete deactivation occurring at about 70°C.

[0041] The dispersible pharmaceutical-based dry powders of the present invention may optionally be combined with pharmaceutical carriers or excipients which are suitable for respiratory and pulmonary administration. Such carriers may serve simply as bulking agents when it is desired to reduce the interferon concentration in the powder which is being delivered to a patient, but may also serve to enhance the stability of the interferon compositions and to improve the dispersibility of the powder within a powder dispersion device in order to provide more efficient and reproducible delivery of the interferon and to improve handling characteristics of the interferon such as flowability and consistency to facilitate manufacturing and powder filling.

[0042] Such carrier materials may be combined with the drug prior to spray drying, i.e., by adding the carrier material to the purified bulk solution. In that way, the carrier particles will be formed simultaneously with the drug particles to produce a homogeneous powder. Alternatively, the carriers may be separately prepared in a dry powder form and combined with the dry powder drug by blending. The powder carriers will usually be crystalline (to avoid water absorption), but might in some cases be amorphous or mixtures of crystalline and amorphous. The size of the carrier particles may be selected to improve the flowability of the drug powder, typically being in the range from 25 µm to 100 µm. A preferred carrier material is crystalline lactose having a size in the above-stated range.

[0043] Alternatively, dry powder compositions may be prepared by other processes such as lyophilization and jet milling as disclosed in WO 91/16038.

TABLE 1

SELECTED MACROMOLECULE DRUGS FOR SYSTEMIC APPLICATIONS	
DRUG	INDICATIONS
Calcitonin	Osteoporosis Prophylaxis Paget's Disease
Erthropoetin (EPO)	Hypercalcemia
Factor IX	Anemia
Granulocyte Colony Stimulating Factor (G-CSF)	Hemophilia B
Granulocyte Macrophage Colony Stimulating Factor (GM-CSF)	Neutropenia
Growth Hormone	Bone Marrow Engraftment/Transplant Failure
Heparin	Short Stature Renal Failure
Heparin (Low Molecular Weight)	Blood Clotting
Insulin	Blood Clotting
Interferon Alpha	Type I and Type II Diabetes
Interferon Beta	Hepatitis B and C Hairy Cell Leukemia Kaposi's Sarcoma
Interferon Gamma	Multiple Sclerosis
Interleukin-2	Chronic Granulomatous Disease
Luteinizing Hormone Releasing Hormone (LHRH)	Renal Cancer
Somatostatin Analog	Prostate Cancer Endometriosis
Vasopressin Analog	Gastrointestinal Cancers
Follicle Stimulating Hormone (FSH)	Diabetes Insipidus Bed Wetting
Amylin	Fertility
Ciliary Neurotrophic Factor	Type I Diabetes
Growth Hormone Releasing Factor (GRF)	Lou Gehrig's Disease
Insulin-Like Growth Factor	Short Stature
Insulinotropin	Osteoporosis Nutritional Support
Interferon Beta	Type II Diabetes
Interferon Gamma	Hepatitis B and C
Interleukin-1 Receptor Antagonist	Rheumatoid Arthritis
Interleukin-3	Rheumatoid Arthritis
Interleukin-4	Adjuvant to Chemotherapy
Interleukin-6	Immunodeficiency Disease
Macrophage Colony Stimulating	Thrombocytopenia
	Fungal Disease

TABLE 1 (continued)

SELECTED MACROMOLECULE DRUGS FOR SYSTEMIC APPLICATIONS	
DRUG	INDICATIONS
Factor (M-CSF)	Cancer Hypercholesterolemia
Nerve Growth Factor	Peripheral Neuropathies
Parathyroid Hormone	Osteoporosis
Somatostatin Analog	Refractory Diarrheas
Thymosin Alpha 1	Hepatitis B and C
IIb/IIIa Inhibitor	Unstable Angina
Alpha-1 Antitrypsin	Cystic Fibrosis
Anti-RSV Antibody	Respiratory Syncytial Virus
Cystic Fibrosis Transmembrane Regulator (CFTR) Gene	Cystic Fibrosis
Deoxyribonuclease (DNase)	Chronic Bronchitis
Heparin	Asthma
Bactericidal/Permeability Increasing Protein (BPI)	Adult Respiratory Distress Syndrome (ARDS)
Anti-CMV Antibody	Cytomegalovirus
Interleukin-1 Receptor	Asthma

SELECTED NON-MACROMOLECULE DRUGS FOR SYSTEMIC AND LOCAL LUNG APPLICATIONS	
DRUG	INDICATIONS
Pentamidine isethiouate	Pneumocystis carini pneumonia
Albuterol sulfate	Bronchospasm
Metaproterenol sulfate	Bronchial asthma
Beclomethasone diprepionate	
Triamcinolone acetamide	
Budesonide acetonide	
Ipratropium bromide	
Flunisolide	
Cromolyn sodium	
Ergotamine Tartrate	Migraines

[0044] The following examples are offered by way of illustration and not limitation.

#### EXPERIMENTAL

[0045] According to the subject invention, the following dispersible dry powder formulations were prepared as described. All compositions produced according to the present invention meet the strict specifications for content and purity required of pharmaceutical products.

#### EXAMPLE I

##### 20.0% INSULIN FORMULATION FOR PULMONARY DELIVERY

##### A. Formulation.

[0046] Bulk crystalline human zinc insulin, was obtained from Eli Lilly and Company, Indianapolis, IN. A 20% insulin formulation was achieved by combining 1.5 mg insulin per 1.0 mL deionized water with 4.96 mg/mL USP mannitol and

1.04 mg/mL citrate buffer (sodium citrate dihydrate USP and citric acid monohydrate USP) for a total solids concentration of 7.5 mg/mL at pH  $6.7 \pm 0.3$ .

#### B. Spray Drying.

[0047] A dry powder of the 20% insulin formulation described above was produced by spray drying the aqueous mixture using a Buchi Laboratory Spray Dryer under the following conditions:

Temperature of aqueous mixture	2-8°C
Inlet temperature	120-122°C
Feed rate	5.3 mL/min
Outlet temperature	80-81°C

[0048] Once the aqueous mixture was consumed, the outlet temperature was maintained at  $< 80^{\circ}\text{C}$  for about 10 minutes by slowly decreasing the inlet temperature to provide a secondary drying.

#### C. Characterization.

[0049] The above 20% insulin dry powder composition contained 66.1% mannitol and 13.9% citrate. The composition was found to contain 1.1 to 2.0% moisture as measured by a coulombic Karl Fischer method using a Mitsubishi CA-06 Moisture Meter.

[0050] The particle size distribution of the composition was measured by liquid centrifugal sedimentation in a Horiba CAPA-700 Particle Size Analyzer following dispersion of the powder on Sedisperse A-11 (Micrometrics, Norcross, GA) and was determined to be  $1.3\text{ }\mu\text{m}$  to  $1.5\text{ }\mu\text{m}$  MMD.

[0051] The delivered dose of the insulin powder composition was measured by collecting the aerosol powder produced by a dry powder dispersion device, similar to devices described in co-pending U.S. Application Serial Numbers 07/910,048; 08/313,707; 08/309,691 and PCT/US92/05621, the disclosures of which are hereby incorporated by reference, on a filter placed over the device mouthpiece. The delivered dose of the insulin powder composition was determined to be  $563 \pm 16\text{ }\mu\text{g}$  or 60 to 64% of the total powder (5.0 mg) loaded into the device.

[0052] The aerosol particle size distribution, measured using a cascade impactor (California Measurements IMPAQ-6), was determined to be  $2.0\text{ }\mu\text{m}$  MMAD, with 86% to 90% of the particles  $< 5.0\text{ }\mu\text{m}$  in diameter.

[0053] The insulin content of the powder, measured by reverse phase HPLC (rpHPLC), was determined to be  $197\text{ }\mu\text{g/mg}$  powder, accounting for 99% of the expected insulin. No degradation peaks were detected in the chromatogram.

### EXAMPLE II

#### 5.0% PARATHYROID HORMONE FORMULATION FOR PULMONARY DELIVERY

##### A. Formulation.

[0054] Bulk 34 amino acid active fragment of parathyroid hormone, PTH (1-34), was obtained from BACHEM CALIFORNIA, Torrance, CA. A 5.0% PTH (1-34) formulation was achieved by combining 0.375 mg PTH (1-34) per 1.0 mL deionized water with 6.06 mg/mL mannitol USP and 1.04 mg/mL citrate buffer (sodium citrate dihydrate USP and citric acid monohydrate USP) for a total solids concentration of 7.48 mg/mL at pH 6.3.

##### B. Spray Drying.

[0055] A dry powder of the 5.0% PTH (1-34) formulation described above was produced by spray drying the aqueous mixture using a Buchi Laboratory Spray Dryer under the following conditions:

Temperature of aqueous mixture	2-8°C
Inlet temperature	122-124°C
Feed rate	5.2 mL/min
Outlet temperature	73-74°C

[0056] Once the aqueous mixture was consumed, the outlet temperature was maintained at  $< 80^{\circ}\text{C}$  for about 5 min-



utes by slowly decreasing the inlet temperature to provide a secondary drying.

### C. Characterization.

[0057] The following characterization of the dry powder formulation described above was carried out using the methods described in Example I unless indicated otherwise.

[0058] The above 5.0% PTH (1-34) dry powder composition contained 81.0% mannitol and 13.9% citrate. The formulation contained 0.5% moisture.

[0059] The particle size distribution of the composition was determined to be 2.4  $\mu\text{m}$  and 2.7  $\mu\text{m}$  MMD in separate measurements.

[0060] The delivered dose of the PTH (1-34) powder was determined to be 161  $\mu\text{g}$  or 64.5% and 175  $\mu\text{g}$  or 69.2% in separate measurements.

[0061] The PTH (1-34) content of the powder, measured by rpHPLC was determined to be 48.5  $\mu\text{g}/\text{mg}$  powder, accounting for 97% of the expected value. No degradation peaks were detected in the chromatogram.

## EXAMPLE III

### 0.7% INTERLEUKIN-1 RECEPTOR FORMULATION FOR PULMONARY DELIVERY

#### A. Formulation.

[0062] Bulk interleukin-1 receptor, IL-1 receptor, was obtained from Immunex Corporation, Seattle, WA. A 0.7% IL-1 receptor formulation was achieved by combining 0.053 mg IL-1 receptor per 1.0 mL deionized water with 7.07 mg/mL raffinose (Pfanstiehl, Waukegan, IL) and 0.373 mg/mL Tris buffer at pH 7.18.

#### B. Spray Drying.

[0063] A dry powder of the 0.7% IL-1 receptor formulation described above was produced by spray drying the aqueous mixture using a Buchi Laboratory Spray Dryer under the following conditions:

Temperature of aqueous mixture	2-8°C
Inlet temperature	135-137°C
Feed rate	4.9 mL/min
Outlet temperature	92-93°C

[0064] Once the aqueous mixture was consumed, the outlet temperature was maintained at 90°C for about 15 minutes by slowly decreasing the inlet temperature to provide a secondary drying.

#### C. Characterization.

[0065] The following characterization of the dry powder formulation described above was carried out using the methods described in Example I unless indicated otherwise.

[0066] The above 0.7% IL-1 receptor dry powder composition contained 94.3% raffinose and 5.0% Tris. The formulation contained  $1.84 \pm 0.25\%$  moisture.

[0067] The particle size distribution of the composition was determined to be 1.95  $\mu\text{m}$  MMD with 100% of the particles < 5.0  $\mu\text{m}$ .

[0068] The delivered dose of the IL-1 receptor powder was determined to be  $22.3 \pm 2.0 \mu\text{g}$  or  $53.4 \pm 4.7\%$ .

[0069] The aerosol particle size distribution, was determined to be 3.2  $\mu\text{m}$  MMAD, with 77% of the particles < 5.0  $\mu\text{m}$  in diameter.

[0070] The IL-1 receptor content of the powder as measured by rpHPLC was determined to be 8.4  $\mu\text{g}/\text{mg}$ , accounting for 120% of the expected IL-1 receptor. No degradation peaks were detected in the chromatogram.

**EXAMPLE IV****5.0% INTERLEUKIN-1 RECEPTOR FORMULATION FOR PULMONARY DELIVERY****A. Formulation.**

[0071] Bulk interleukin-1 receptor, IL-1 receptor, was obtained from Immunex Corporation, Seattle, WA. A 5.0% IL-1 receptor formulation was achieved by combining 0.375 mg IL-1 receptor per 1.0 mL deionized water with 6.77 mg/mL raffinose and 0.351 mg/mL Tris buffer at pH 7.35.

**B. Spray Drying.**

[0072] A dry powder of the 5.0% IL-1 receptor formulation described above was produced by spray drying the aqueous mixture using a Buchi Laboratory Spray Dryer under the following conditions:

Temperature of aqueous mixture	2-8°C
Inlet temperature	138°C
Feed rate	4.9 mL/min
Outlet temperature	91°C

[0073] Once the aqueous mixture was consumed, the outlet temperature was maintained at 90°C for about 15 minutes by slowly decreasing the inlet temperature to provide a secondary drying.

**C. Characterization.**

[0074] The following characterization of the dry powder formulation described above was carried out using the methods described in Example I unless indicated otherwise.

[0075] The above 5.0% IL-1 receptor dry powder composition contained 90.3% raffinose and 4.7% Tris. The formulation contained  $1.75 \pm 0.26\%$  moisture.

[0076] The particle size distribution of the composition was determined to be 2.74  $\mu\text{m}$  MMD with 97% of the particles < 5.0  $\mu\text{m}$ .

[0077] The delivered dose of the IL-1 receptor powder was determined to be  $123.4 \pm 24.5 \mu\text{g}$  or  $49.3 \pm 9.8\%$ .

[0078] The aerosol particle size distribution, was determined to be 4.1  $\mu\text{m}$  MMAD, with 64% of the particles < 5.0  $\mu\text{m}$  in diameter.

[0079] The IL-1 receptor content of the powder as measured by rpHPLC was determined to be  $52.7 \pm 1.8 \mu\text{g/mg}$ , accounting for 105% of the expected IL-1 receptor. No degradation peaks were detected in the chromatogram.

**EXAMPLE V****26.7% HUMAN CALCITONIN FORMULATION FOR PULMONARY DELIVERY****A. formulation.**

[0080] Bulk human calcitonin was obtained from Ciba-Geigy. A 26.7% human calcitonin formulation was achieved by combining 1.9 mg human calcitonin per 1.0 mL deionized water with 4.3 mg/mL mannitol and 0.9 mg/mL citrate buffer at pH 3.85.

**B. Spray Drying.**

[0081] A dry powder of the 26.7% human calcitonin formulation described above was produced by spray drying the aqueous mixture using a Buchi Laboratory Spray Dryer under the following conditions:

Temperature of aqueous mixture	4°C
Inlet temperature	119°C
Feed rate	5.5 mL/min
Outlet temperature	78°C

(continued)

Atomizer coolant temperature	0-5°C
Cyclone coolant temperature	25-30°C

[0082] Once the aqueous mixture was consumed, the outlet temperature was maintained at 80°C for about 10 minutes by slowly decreasing the inlet temperature to provide a secondary drying.

#### C. Characterization.

[0083] The following characterization of the dry powder formulation described above was carried out using the methods described in Example I unless indicated otherwise.

[0084] The above 26.7% human calcitonin dry powder composition contained 60% mannitol and 13.3% citrate. The formulation contained 0.71% moisture.

[0085] The particle size distribution of the composition was determined to be  $1.33 \pm 0.63 \mu\text{m}$  MMD.

[0086] The delivered dose of the human calcitonin powder was determined to be  $76.8 \pm 6.7\%$ .

[0087] The human calcitonin content of the powder as measured by rpHPLC was determined to be 272.0  $\mu\text{g}/\text{mg}$ , accounting for  $102 \pm 1.7\%$  of the expected human calcitonin. No degradation peaks were detected in the chromatogram.

### EXAMPLE VI

#### 90% ALPHA-1 ANTITRYPSIN FORMULATION FOR PULMONARY DELIVERY

##### A. Formulation.

[0088] Bulk alpha-1 antitrypsin, A1A, was obtained from Armour Pharmaceutical Company, Kankakee, IL. A 90% A1A formulation was achieved by combining 4.89 mg A1A per 1.0 mL deionized water with 0.54 mg/mL citrate buffer at pH 6.0.

##### B. Spray Drying.

[0089] A dry powder of the 90% A1A formulation described above was produced by spray drying the aqueous mixture using a Buchi Laboratory Spray Dryer under the following conditions:

Temperature of aqueous mixture	4°C
Inlet temperature	98-101°C
Feed rate	5.0 mL/min
Outlet temperature	65°C
Atomizer coolant temperature	2-8°C
Cyclone coolant temperature	30°C

[0090] Once the aqueous mixture was consumed, the outlet temperature was maintained at 69°C for about 10 minutes by slowly decreasing the inlet temperature to provide a secondary drying.

##### C. Characterization.

[0091] The following characterization of the dry powder formulation described above was carried out using the methods described in Example I unless indicated otherwise.

[0092] The above 90% A1A dry powder composition contained 10.0% citrate. The formulation contained 4.79% moisture.

[0093] The particle size distribution of the composition was determined to be  $1.71 \pm 0.87 \mu\text{m}$  MMD.

[0094] The delivered dose of the 90% A1A powder was determined to be  $67.0 \pm 5.0\%$ .

[0095] The aerosol particle size distribution, was determined to be 1.0  $\mu\text{m}$  MMAD, with 90% of the particles < 5.0  $\mu\text{m}$  in diameter.

[0096] The A1A content of the powder as measured by rpHPLC was determined to be 80% of the expected value. No degradation peaks were detected in the chromatogram. The activity after spray drying was determined to be  $74 \pm 1\%$

**EXAMPLE VII****0.3% BETA INTERFERON FORMULATION FOR PULMONARY DELIVERY CONTAINING HUMAN SERUM ALBUMIN****A. Formulation.**

[0097] Bulk beta interferon, IFN- $\beta$ , was obtained from Toray Industries, Inc., Tokyo, Japan. A 0.3% IFN- $\beta$  formulation was achieved by combining 0.025 mg IFN- $\beta$  per 1.0 mL deionized water with 5.54 mg/mL human serum albumin (HSA), 2.3 mg/mL citrate buffer and 0.345 mg/mL of NaCl at pH 4.5.

**B. Spray Drying.**

[0098] A dry powder of the 0.3% IFN- $\beta$  formulation described above was produced by spray drying the aqueous mixture using a Buchi Laboratory Spray Dryer under the following conditions:

Temperature of aqueous mixture	2-8°C
Inlet temperature	93°C
Feed rate	2.7 mL/min
Outlet temperature	62°C

**C. Characterization.**

[0099] The following characterization of the dry powder formulation described above was carried out using the methods described in Example I unless indicated otherwise.

[0100] The above 0.3% IFN- $\beta$  dry powder composition contained 66.0% HSA, 27.4% citrate, 4.1% NaCl. The formulation contained 4.22% moisture.

[0101] The particle size distribution of the composition was determined to be 1.62  $\mu$ m MMD with 94.8% of the particles < 5  $\mu$ m.

[0102] The delivered dose of the 0.3% IFN- $\beta$  powder was determined to be 9.9  $\mu$ g/mg or 66.0  $\pm$  4.0%.

[0103] The aerosol particle size distribution, was determined to be 2.0  $\mu$ m MMAD, with 85% of the particles < 5.0  $\mu$ m in diameter.

[0104] The IFN- $\beta$  activity of the powder as measured by IFN- $\beta$  enzyme immunoassay (Toray-Fuji Bionics) and was determined to be 109  $\pm$  8% of the expected activity.

**EXAMPLE VIII****0.3% BETA INTERFERON FORMULATION FOR PULMONARY DELIVERY CONTAINING RAFFINOSE****A. Formulation.**

[0105] Bulk beta interferon, IFN- $\beta$ , was obtained from Toray Industries, Inc., Tokyo, Japan. A 0.3% IFN- $\beta$  formulation was achieved by combining 0.025 mg IFN- $\beta$  per 1.0 mL deionized water with 4.7 mg/mL raffinose, 1.0 mg/mL human serum albumin (HSA), 2.3 mg/mL citrate buffer and 0.3 mg/mL of NaCl at pH 4.5.

**B. Spray Drying.**

[0106] A dry powder of the 0.3% IFN- $\beta$  formulation described above was produced by spray drying the aqueous mixture using a Buchi Laboratory Spray Dryer under the following conditions:

Temperature of aqueous mixture	2-8°C
Inlet temperature	145°C
Feed rate	5.0 mL/min
Outlet temperature	87°C

[0107] Once the aqueous mixture was consumed, the outlet temperature was maintained at 97°C for about 5 minutes

by slowly decreasing the inlet temperature to provide a secondary drying.

#### C. Characterization.

[0108] The following characterization of the dry powder formulation described above was carried out using the methods described in Example I unless indicated otherwise.

[0109] The above 0.3% IFN- $\beta$  dry powder composition contained 56.4% raffinose, 11.9% HSA, 27.4% citrate, 3.5% NaCl. The formulation contained 0.69% moisture.

[0110] The particle size distribution of the composition was determined to be 2.06  $\mu\text{m}$  MMD with 88.9% of the particles < 5  $\mu\text{m}$ .

[0111] The delivered dose of the 0.3% IFN- $\beta$  powder was determined to be 10.2  $\mu\text{g}/\text{mg}$  or  $68.0 \pm 2.0\%$ .

[0112] The aerosol particle size distribution, was determined to be 2.5  $\mu\text{m}$  MMAD, with 84% of the particles < 5.0  $\mu\text{m}$  in diameter.

[0113] The IFN- $\beta$  activity of the powder as measured by IFN- $\beta$  enzyme immunoassay (Toray-Fuji Bionics) and was determined to be  $109 \pm 8\%$  of the expected activity.

#### EXAMPLE IX

##### **93% LOW MOLECULAR WEIGHT HEPARIN FORMULATION FOR PULMONARY DELIVERY**

#### A. Formulation.

[0114] Bulk low molecular weight heparin sodium salt (Av. Mol. Wt.: Approx. 6000) from porcine intestinal mucosa, heparin (LMW), was obtained from Sigma Chemical, St. Louis, MO.. A 93% heparin (LMW) formulation was achieved by combining 6.9 mg heparin (LMW) per 1.0 mL deionized water with 0.5 mg/mL HSA at pH 6.9.

#### B. Spray Drying.

[0115] A dry powder of the 93% heparin (LMW) formulation described above was produced by spray drying the aqueous mixture using a Buchi Laboratory Spray Dryer under the following conditions:

Temperature of aqueous mixture	2-8°C
Inlet temperature	140°C
Feed rate	3.8 mL/min
Outlet temperature	85°C
Atomizer coolant temperature	2-8°C
Cyclone coolant temperature	20°C

[0116] Once the aqueous mixture was consumed, the outlet temperature was maintained at 80°C for about 10 minutes by slowly decreasing the inlet temperature to provide a secondary drying.

#### C. Characterization.

[0117] The following characterization of the dry powder formulation described above was carried out using the methods described in Example I unless indicated otherwise.

[0118] The above 93% heparin (LMW) dry powder composition contained 7.0% HSA.

[0119] The delivered dose of the 93% heparin (LMW) powder was determined to be  $60.0 \pm 1.0\%$ .

[0120] The aerosol particle size distribution, was determined to be 3.5  $\mu\text{m}$  MMAD, with 70% of the particles < 5.0  $\mu\text{m}$  in diameter.

#### EXAMPLE X

##### **97% UNFRACTIONATED HEPARIN FORMULATION FOR PULMONARY DELIVERY**

#### A. Formulation.

[0121] Bulk unfractionated heparin sodium salt from porcine intestinal mucosa, heparin, was obtained from Sigma

Chemical, St. Louis, MO. A 97% heparin formulation was achieved by combining 7.0 mg heparin per 1.0 mL deionized water with 0.25 mg/mL HSA at pH 6.55.

#### B. Spray Drying.

[0122] A dry powder of the 97% heparin formulation described above was produced by spray drying the aqueous mixture using a Buchi Laboratory Spray Dryer under the following conditions:

Temperature of aqueous mixture	2-8°C
Inlet temperature	150°C
Feed rate	4.0 mL/min
Outlet temperature	85°C
Atomizer coolant temperature	2-8°C
Cyclone coolant temperature	20°C

[0123] Once the aqueous mixture was consumed, the outlet temperature was maintained at 80°C for about 10 minutes by slowly decreasing the inlet temperature to provide a secondary drying.

#### C. Characterization.

[0124] The following characterization of the dry powder formulation described above was carried out using the methods described in Example I unless indicated otherwise.

[0125] The above 97% heparin dry powder composition contained 3.0% HSA. The formulation contained 5.11% moisture.

[0126] The particle size distribution of the composition was determined to be 2.0 to 2.5 µm MMD.

[0127] The delivered dose of the 97% heparin powder was determined to be  $79.0 \pm 6.0\%$ .

[0128] The aerosol particle size distribution, was determined to be 3.2 µm MMAD, with 70% of the particles < 5.0 µm in diameter.

### EXAMPLE XI

#### LIPID VECTOR GENE FORMULATION FOR PULMONARY DELIVERY

##### A. Formulation.

[0129] Bulk pCMVβ DNA:Lipid vector was obtained from Genzyme Corporation, Cambridge, MA. A 0.71% DNA:Lipid vector formulation was achieved by combining 0.005:0.03 mg DNA:Lipid vector per 1.0 mL deionized water with 5.3 mg/mL glycine (J.T. Baker) 0.3 mg/mL HSA at pH 6.4.

##### B. Spray Drying.

[0130] A dry powder of the DNA:Lipid vector formulation described above was produced by spray drying the aqueous mixture using a Buchi Laboratory Spray Dryer under the following conditions:

Temperature of aqueous mixture	2-8°C
Inlet temperature	120°C
Feed rate	3.8 mL/min
Outlet temperature	71°C
Atomizer coolant temperature	2-8°C
Cyclone coolant temperature	2-8°C

[0131] Once the aqueous mixture was consumed, the outlet temperature was maintained at 65°C for about 5 minutes by slowly decreasing the inlet temperature to provide a secondary drying.

C. Characterization.

[0132] The following characterization of the dry powder formulation described above was carried out using the methods described in Example I unless indicated otherwise.

[0133] The above 0.71% DNA:Lipid vector dry powder composition contained 93.97% glycine, and 5.32% HSA.

[0134] The particle size distribution of the composition was determined to be 2.0  $\mu\text{m}$  MMD.

[0135] The delivered dose of the 97% heparin (HMW) powder was determined to be  $64.0 \pm 1.0\%$ .

[0136] The aerosol particle size distribution, was determined to be 2.4  $\mu\text{m}$  MMAD, with 75% of the particles < 5.0  $\mu\text{m}$  in diameter.

[0137] Activity after spray drying was determined to be 160% of the expected value.

**EXAMPLE XII****ADENOVIRAL VECTOR GENE FORMULATION FOR PULMONARY DELIVERY**A. Formulation.

[0138] Bulk pCMV $\beta$  DNA:Adenovirous vector was obtained from Genzyme Corporation, Cambridge, MA. A DNA:adenovirous vector formulation was achieved by combining 108 PFU/mL DNA:Lipid vector per 1.0 mL deionized water with 6.1 mg/mL glycine J.T. Baker) 2.5 mg/mL HSA, 1.9 mg/mL phosphate buffer at pH 7.4.

B. Spray Drying.

[0139] A dry powder of the DNA:Lipid vector formulation described above was produced by spray drying the aqueous mixture using a Buchi Laboratory Spray Dryer under the following conditions:

Temperature of aqueous mixture	2-8°C
Inlet temperature	105°C
Feed rate	2.9 mL/min
Outlet temperature	72°C
Atomizer coolant temperature	2-8°C
Cyclone coolant temperature	20°C

[0140] Once the aqueous mixture was consumed, the outlet temperature was maintained at 70°C for about 10 minutes by slowly decreasing the inlet temperature to provide a secondary drying.

C. Characterization.

[0141] The following characterization of the dry powder formulation described above was carried out using the methods described in Example I unless indicated otherwise.

[0142] The above DNA:adenovirous vector dry powder composition contained 58% glycine, and 24% HSA and 18% phosphate buffer.

[0143] The particle size distribution of the composition was determined to be 2.3  $\mu\text{m}$  MMD.

[0144] The delivered dose of the 97% heparin (HMW) powder was determined to be  $51.0 \pm 1.0\%$ .

[0145] The aerosol particle size distribution, was determined to be 1.8  $\mu\text{m}$  MMAD, with 80% of the particles < 5.0  $\mu\text{m}$  in diameter.

[0146] Activity after spray drying was determined to be 76% of the expected value.

[0147] All publications and patent applications mentioned in this specification are herein incorporated by reference to the same extent as if each individual publication or patent application was specifically and individually indicated to be incorporated by reference.

[0148] The invention now being fully described, it will be apparent to one of ordinary skill in the art that many changes and modifications can be made thereto without departing from the spirit or scope of the appended claims.

**Claims**

1. A spray-dried pharmaceutical-based dispersible dry powder composition for pulmonary delivery, comprising:

a therapeutically effective amount of a macromolecule; and  
a pharmaceutically acceptable carrier with the provisos that:

- (i) the carrier is neither hydroxypropylcellulose or hydroxypropylmethylcellulose; and
  - (ii) the macromolecule is neither insulin nor an interferon.
2. The composition of claim 1, wherein the macromolecule is selected from the group consisting of calcitonins, erythropoietin, factor IX, G-CSF, GM-CSF, growth hormone, heparin, low molecular weight heparin, interleukin-2, LHRH, somatostatin analog, vasopressin analog, amylin, ciliary neurotrophic factor, interleukin-3, interleukin-4, M-CSF, nerve growth factor, parathyroid hormone, thymosin alpha-1, IIb/IIIa inhibitor, alpha-1 antitrypsin, anti-RSV antibody, CFTR gene, DNase, BPI protein, anti-CMV antibody, interleukin-1 receptor and nucleic acids.
3. The composition of claim 1 or claim 2, wherein the macromolecule is selected from the group consisting of interleukin 1 receptor, parathyroid hormone, alpha-1 antitrypsin, low molecular weight heparin, and nucleic acids.
4. The composition of any one of claims 1 to 3, wherein the macromolecule is a nucleic acid.
5. The composition of any one preceding claim wherein said carrier is selected from the group consisting of (i) human serum albumin, (ii) carbohydrates selected from the group consisting of monosaccharides, disaccharides, cyclodextrins, maltodextrins, raffinose and alditols, (iii) amino acids and (iv) polypeptides.
6. The composition of any one of claims 1 to 5, wherein said carrier is selected from the group consisting of galactose, D-mannose, sorbose, lactose, trehalose, 2-hydroxypropyl- $\beta$ -cyclodextrin, raffinose, mannitol, and xylitol.
7. The composition of any one of claims 1 to 5, wherein said carrier is an amino acid.
8. The composition of any one preceding claim wherein said carrier is substantially free from penetration enhancers.
9. The composition of any one preceding claim, wherein said composition further comprises a hydrophobic amino acid.
10. The composition of claim 9, wherein said hydrophobic amino acid is selected from the group consisting of tryptophan, tyrosine, leucine, and phenylalanine.
11. The composition of any preceding claim comprising particles having a uniform distribution of macromolecule and carrier.
12. The composition of any one preceding claim comprising particles having a diameter less than 10 microns.
13. The composition of any one preceding claim, wherein 95% of the mass of the composition comprises particles having a particle size below 10 microns.
14. The composition of any one preceding claim comprising particles of a size ranging from 1.0-5.0 microns mass median diameter (MMD).
15. The composition of any one preceding claim comprising particles of a size ranging from 1.0-4.0 microns mass median diameter (MMD).
16. The composition of any one preceding claim comprising particles having an aerosol particle size distribution from 1.0-5.0 microns mass median aerodynamic diameter (MMAD).
17. The composition of any one preceding claim comprising particles having an aerosol particle size distribution from 1.5-4.0 microns mass median aerodynamic diameter (MMAD).
18. The composition of any one preceding claim comprising particles **characterized by** a delivered dose of greater than 30%.
19. The composition of any one preceding claim **characterized by** a delivered dose of greater than 60%.



20. The composition of any one preceding claim having a homogeneous constitution.
21. The composition of any one preceding claim comprising less than 5% degradation products.
- 5 22. The composition of any one preceding claim which, when pulmonarily administered to a subject, rapidly dissolves in the fluid layer of the alveolar lining of the lung.
23. The composition of any one preceding claim having a moisture content below 10% by weight.
- 10 24. The composition of any one preceding claim, wherein said macromolecule, when administered by inhalation, is systemically absorbed in a rapid manner.
25. An aerosolized dry powder composition as defined in any one preceding claim.
- 15 26. A unit dosage form for pulmonary delivery of a macromolecule-based composition, comprising a unit dosage receptacle containing the dry powder composition according to any one of claims 1 to 24.
27. A method for aerosolizing a pharmaceutical-based dry powder composition comprising:  
20       dispersing an amount of a composition according to any one of claims 1 to 24 in a gas stream to form an aerosol and  
          capturing the aerosol in a chamber suitable for subsequent inhalation of the aerosol by a patient.
28. A method for preparing a composition as defined in any one of claims 1 to 24, said method comprising:  
25       providing an aqueous mixture of the macromolecule and the pharmaceutically acceptable carrier; and  
          spray-drying the mixture under conditions effective to produce said composition.
29. The method of claim 28, wherein said aqueous mixture of the macromolecule and the carrier is a homogeneous  
30       aqueous mixture.
30. The method of claim 29, wherein said aqueous mixture of the macromolecule and the carrier is a solution.
31. The method of any one of claims 28 to 30, wherein the spray-dried respirable powder produced in said spray-  
35       drying step, when administered pulmonarily to a patient in need thereof, permits the macromolecule to be system-  
          ically absorbed in a rapid manner.
32. A composition as defined in any one of claims 1 to 24 for use in a method of pulmonary administration so as to  
40       treat a condition responsive to treatment with said macromolecule.
33. Use of a composition as defined in any one of claims 1 to 24 in the manufacture of a medicament for use in a  
      method of pulmonary administration so as to treat a condition responsive to treatment with said macromolecule.
34. A dispersible pharmaceutical-based dry powder composition for pulmonary delivery, said composition comprising  
45       a therapeutically effective amount of a pharmaceutical in combination with a pharmaceutically acceptable carrier,  
      wherein the composition comprises particles and wherein 95% of the mass of the composition comprises particles  
      having a particle size below 10  $\mu\text{m}$ .
35. A dispersible pharmaceutical-based dry powder composition for pulmonary delivery, said composition comprising  
50       a therapeutically effective amount of a macromolecule selected from the group consisting of interleukin 1 receptor,  
      heparin, low molecular weight heparin, and calcitonin, in combination with pharmaceutically acceptable carrier.
36. The composition of claim 34 or 35, wherein the composition is substantially free from penetration enhancers.
- 55 37. The composition of claim 35 or 36, wherein the carrier comprises HSA.
38. The composition of claim 36 or 37, wherein the carrier further comprises a carbohydrate bulking agent.

39. The composition of claim 34 or 35, wherein about 95% of the mass of the dry powder composition has a particle size of less than 10  $\mu\text{m}$ .
- 5 40. The composition of claim 34 or 39, wherein about 80% of the mass of the dry powder composition has a particle size of less than 5  $\mu\text{m}$ .
- 10 41. The composition of claim 34, wherein the pharmaceutical comprises a macromolecule selected from the group consisting of insulin, interleukin 1 receptor, parathyroid hormone alpha-1 antitrypsin, calcitonin, low molecular weight heparin, and nucleic acids.
- 15 42. A unit dosage form for pulmonary delivery of a pharmaceutical, which dosage form comprises a unit dosage receptacle containing a dispersible pharmaceutical-based dry powder composition, which composition comprises a therapeutically effective amount of the pharmaceutical in combination with a pharmaceutically acceptable carrier according to any of claims 34-41.
- 20 43. A method of treating a disease state responsive to treatment by a pharmaceutical, which method comprises pulmonarily administering to a subject in need thereof a physiologically effective amount of a dispersible pharmaceutical-based dry powder composition according to any of claims 34-41.
- 25 44. A method for aerosolizing a pharmaceutical-based dry powder composition that comprises a therapeutically effective amount of the pharmaceutical in combination with a pharmaceutically acceptable carrier, which method comprises:
- dispersing an amount of a dry powder composition according to any of claims 34-41 in a gas stream to form an aerosol; and
- capturing the aerosol in a chamber suitable for subsequent inhalation by a patient.
- 30 45. A method for preparing a spray-dried, pharmaceutical-based dry powder that comprises a therapeutically effective amount of a pharmaceutical and a pharmaceutically acceptable carrier, which method comprises spray drying an aqueous mixture of the pharmaceutical and the carrier under conditions to provide a respirable dry powder comprising particles wherein 95% of the mass of the composition comprises particles having a particle size below 10  $\mu\text{m}$ .
- 35 46. A method for preparing a spray-dried, pharmaceutical-based dry powder composition that comprises a therapeutically effective amount of a pharmaceutical and a pharmaceutically acceptable carrier, which method comprises spray drying an aqueous mixture of a pharmaceutical selected from the group consisting of parathyroid hormone, interleukin 1 receptor, heparin, low molecular weight heparin, and calcitonin.
- 40 47. The method of claim 45 or 46, wherein the carrier comprises HSA.
48. The method of claim 47, wherein the carrier further comprises a carbohydrate bulking agent.
49. The method of claim 48, wherein the bulking agent is mannitol.
- 45 50. The method of claim 45, wherein 80% of the mass of the spray-dry composition has a particle size less than 5  $\mu\text{m}$ .
- 50 51. A spray-dried, macromolecule-based dry powder composition for pulmonary delivery, said composition comprising a therapeutically effective amount of the macromolecule in combination with a pharmaceutically acceptable carrier produced by the method of claims 45-50.
- 55 52. Compositions as in claims 34-41, having a moisture content below 10%.



European Patent  
Office

# PARTIAL EUROPEAN SEARCH REPORT

Application Number

which under Rule 45 of the European Patent Convention EP 04 07 5809  
shall be considered, for the purposes of subsequent  
proceedings, as the European search report

DOCUMENTS CONSIDERED TO BE RELEVANT			
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (Int.Cl.7)
X	WO 95/00128 A (ASTRA AKTIEBOLAGET) 5 January 1995 (1995-01-05)	1-3,5,8, 11-34, 36, 39-46, 50-52	A61K9/00 A61K9/16
Y	* claims 1,3-5,11,12,17-19 * * page 10, line 10 - line 12 * * page 14, line 18 - line 26 * * page 17; example 2; table 1 * ---	37,38, 47-49	
X	EP 0 606 486 A (TEIJIN LIMITED) 20 July 1994 (1994-07-20)	1,2,5-8, 11-34, 36,39, 40, 42-45, 50-52	
Y	* claims 1,11,12 * * page 8, line 5 - line 17 * * page 11; example 7; table 1 * * page 12, line 31 - line 37 * ---	9,10,35	
			TECHNICAL FIELDS SEARCHED (Int.Cl.7)
			A61K
<b>INCOMPLETE SEARCH</b> The Search Division considers that the present application, or one or more of its claims, does/do not comply with the EPC to such an extent that a meaningful search into the state of the art cannot be carried out, or can only be carried out partially, for these claims. Claims searched completely :  Claims searched incompletely :  Claims not searched :  Reason for the limitation of the search: Although claim 43 is directed to a method of treatment of the human/animal body (Article 52(4) EPC), the search has been carried out and based on the alleged effects of the compound/composition.			
Place of search		Date of completion of the search	Examiner
THE HAGUE		21 April 2004	Ventura Amat, A
<b>CATEGORY OF CITED DOCUMENTS</b> X : particularly relevant if taken alone Y : particularly relevant if combined with another document of the same category A : technological background O : non-written disclosure P : intermediate document T : theory or principle underlying the invention E : earlier patent document, but published on, or after the filing date D : document cited in the application L : document cited for other reasons & : member of the same patent family, corresponding document			

EPO FORM 1503 (3.82) (P04C07)



European Patent  
Office

# PARTIAL EUROPEAN SEARCH REPORT

Application Number  
EP 04 07 5809

DOCUMENTS CONSIDERED TO BE RELEVANT			CLASSIFICATION OF THE APPLICATION (Int.Cl.7)
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	
Y	WO 91/16038 A (TORAY) 31 October 1991 (1991-10-31) * claims 1,2,9 * * page 18; example 9 * ---	37,38, 47-49	
Y	WO 90/09781 A (RORER INTERNATIONAL (OVERSEAS)) 7 September 1990 (1990-09-07) * claims 1,7,8,11-13 * * page 5, line 1 - page 6, line 2 * * examples 1-5 * -----	9,10,35	
			TECHNICAL FIELDS SEARCHED (Int.Cl.7)

EPO FORM 1503 03.92 (P04C10)

**ANNEX TO THE EUROPEAN SEARCH REPORT  
ON EUROPEAN PATENT APPLICATION NO.**

EP 04 07 5809

This annex lists the patent family members relating to the patent documents cited in the above-mentioned European search report.  
The members are as contained in the European Patent Office EDP file on  
The European Patent Office is in no way liable for these particulars which are merely given for the purpose of information.

21-04-2004

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
WO 9500128      A	05-01-1995	AT 183920 T	15-09-1999
		AT 206046 T	15-10-2001
		AU 692780 B2	18-06-1998
		AU 7090194 A	17-01-1995
		AU 692781 B2	18-06-1998
		AU 7090294 A	17-01-1995
		BR 9406907 A	02-04-1996
		BR 9406908 A	02-04-1996
		CA 2166108 A1	05-01-1995
		CA 2166109 A1	05-01-1995
		CN 1127471 A ,B	24-07-1996
		CN 1129904 A ,B	28-08-1996
		CZ 9503393 A3	15-05-1996
		CZ 9503428 A3	15-05-1996
		DE 69420412 D1	07-10-1999
		DE 69420412 T2	13-04-2000
		DE 69428442 D1	31-10-2001
		DE 69428442 T2	11-07-2002
		DK 706382 T3	13-03-2000
		DK 706383 T3	10-12-2001
		EE 3221 B1	15-10-1999
		EE 3222 B1	15-10-1999
		EG 20599 A	30-09-1999
		EG 21484 A	28-11-2001
		EP 0706382 A1	17-04-1996
		EP 0706383 A1	17-04-1996
		ES 2138087 T3	01-01-2000
		ES 2162865 T3	16-01-2002
		FI 956227 A	22-12-1995
		FI 956228 A	22-12-1995
		GR 3031974 T3	31-03-2000
		HK 1009584 A1	14-04-2000
		HK 1009587 A1	03-05-2002
		HU 75065 A2	28-03-1997
		HU 75066 A2	28-03-1997
		IL 110084 A	14-07-1999
		IL 110085 A	14-06-2001
		JP 8512027 T	17-12-1996
		JP 9500621 T	21-01-1997
		LT 1976 A ,B	25-05-1995
		LT 1977 A ,B	31-01-1995
		MX 9404761 A1	31-01-1995
		MX 9404762 A1	31-01-1995
		NO 955226 A	15-02-1996
		NO 955227 A	20-02-1996
		NZ 268137 A	24-10-1997

EPO FORM P0455

For more details about this annex : see Official Journal of the European Patent Office, No. 12/82

**ANNEX TO THE EUROPEAN SEARCH REPORT  
ON EUROPEAN PATENT APPLICATION NO.**

EP 04 07 5809

This annex lists the patent family members relating to the patent documents cited in the above-mentioned European search report.  
The members are as contained in the European Patent Office EDP file on  
The European Patent Office is in no way liable for these particulars which are merely given for the purpose of information.

21-04-2004

Patent document cited in search report		Publication date	Patent family member(s)	Publication date
WO 9500128	A		NZ 268138 A	24-10-1997
			NZ 328475 A	27-04-2001
			NZ 328476 A	28-05-1999
			PL 312205 A1	01-04-1996
-----				
EP 606486	A	20-07-1994	AT 204750 T	15-09-2001
			AU 660824 B2	06-07-1995
			AU 4355593 A	04-01-1994
			CA 2115444 A1	23-12-1993
			DE 69330672 D1	04-10-2001
			DE 69330672 T2	27-06-2002
			EP 0606486 A1	20-07-1994
			JP 2962578 B2	12-10-1999
			KR 208979 B1	15-07-1999
			US 5626871 A	06-05-1997
			AT 222754 T	15-09-2002
			AU 659328 B2	11-05-1995
			AU 4355693 A	04-01-1994
			CA 2115065 A1	23-12-1993
			DE 69332240 D1	02-10-2002
			DE 69332240 T2	10-04-2003
			EP 0611567 A1	24-08-1994
			ES 2159524 T3	16-10-2001
			ES 2177544 T3	16-12-2002
			WO 9325193 A1	23-12-1993
			WO 9325198 A1	23-12-1993
			JP 2907551 B2	21-06-1999
			US 5972388 A	26-10-1999
-----				
WO 9116038	A	31-10-1991	JP 5000963 A	08-01-1993
			AT 155682 T	15-08-1997
			DE 69126935 D1	28-08-1997
			DE 69126935 T2	20-11-1997
			EP 0477386 A1	01-04-1992
			WO 9116038 A1	31-10-1991
-----				
WO 9009781	A	07-09-1990	AU 5194990 A	26-09-1990
			CA 2050905 A1	24-08-1990
			EP 0460064 A1	11-12-1991
			JP 5508616 T	02-12-1993
			NO 913298 A	22-10-1991
			WO 9009781 A1	07-09-1990
-----				

EPO FORM P0459

For more details about this annex : see Official Journal of the European Patent Office, No. 12/82